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# Mumford-Shah based registration

A comparison of a level set and a phase field approach

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**Abstract** Traditionally, different image processing tasks are mainly considered on their own. The main aim of this paper is a combination of *registration* [25, 26, 47, 58–60], i. e., the spatial alignment of images and *segmentation* [19, 53, 17, 18], i. e., the recognition of edges and object contours in images. A proper registration depends on a good initial segmentation and vice versa. In this paper it is proposed to link these problems together by formulating a coupled variational problem. The focus is on edge-based instead of intensity-based methods and a variational model based on the Mumford-Shah free discontinuity problem. In particular this paper is devoted to the comparison of a sharp interface approach with a phase field approach.

# **1** Introduction

In particular on the background of medical applications denoising, segmentation and registration are well established as fundamental problems in image processing. An enormous amount of state-of-the-art imaging methods enables precise studies of the immense *variability* of human anatomy. We refer to the excellent reviews by Miller, Trouvé and Younes [57] and the overview article of Grenander and Miller [44]. Frequently, different images show corresponding structures at usually nonlinearly transformed positions [58,70,51]. As the image modality differs there is also no correlation of image intensities at corresponding positions. But an at least

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partial correspondence of edge sets is feasible. Hence, edge segmentation might help in the registration. On the other hand, integrated knowledge from different image modalities will lead to better segmentation. This circular dependence of registration and edge segmentation is well-known. One might think for example of a pair *magnetic resonance* (MR) and computed tomography (CT) images, or simply a color image instead of a gray scale image. An alternative, global morphological matching approach has been presented by Viola, Wells et al. [74,76] and Collignon et al. [55] based on a information theoretic approach for the registration of multimodal images. Their information theoretic method is based on a maximization of the so called mutual information of images of different modality. In [39] a variational approach not relying on statistics is proposed for morphological matching was presented. Both approaches do not make explicit use of segmentation results.

Here, we focus on the registration of edges. The set of detectable edges in the different images or color channels is often disrupted and irregular. Furthermore they are most often given by binary indicators, hence information about *weak* edges is destroyed and often neglected. Let us first assume that we enrich the image space by overlaying several images, which have been registered perfectly in a preprocessing step. Features which are very weak and hardly visible in one of the images might be clear and salient in the other image. A feature detection model may now exploit the complementary information of both images

On the other hand, if a reliable segmentation of important objects in two images is available, the process of registration can be aided significantly. Mapping the object contours in the reference onto the contours in the template image, significantly simplifies the search space. The deformation is already determined on these boundaries modulo tangential distortion.

Due to this dependency it appears natural to combine both problems into one model. From a more general point of view, this would correspond to a simultaneous detection of image features, that ought to be coupled by a deformation. The subtlety of this approach is that edge contours as well as the deformation are unknowns. The whole process can be described as follows:

Given a pair of images, a reference and a template image, we aim to find a deformation and, simultaneously, a set of edges in the reference image, such that transformed edge set matches the edges in the template image. Furthermore, the deformation itself and the edge sets should be regular.

In this formulation, the deformation is initially only determined on the set itself. Eventually we aim at a smooth extension of this deformation to the rest of the image domain in order to obtain a mapping of the images also away from the feature sets. We are going to ensure smoothness of the deformation and smoothness of the deformed edge set incorporating an elastic variational model for the deformation.

To motivate our approach let us first briefly review the variational approach presented by Mumford and Shah [62] and thereby describe in more mathematical detail what is meant by feature extraction and regularity of the edge set.

Mumford and Shah proposed to consider the following functional

$$E_{MS}[u,\Gamma] = \frac{1}{2} \int_{\Omega} (u-u_0)^2 dx + \frac{\mu}{2} \int_{\Omega \setminus \Gamma} \|\nabla u\|^2 dx + v \mathscr{H}^{n-1}(\Gamma).$$
(1)

The mathematical treatment of this energy is subtle. It has to be minimized over the set of admissible curves  $\Gamma$  and admissible *u* simultaneously. However, it is not possible to obtain lower-semicontinuity of the Hausdorff measure within a reasonable topology of subsets of  $\Omega$ .

The existence theory is established by DE GIORGI, CAR-RIERO AND LEACI [33] who proposed to consider the minimization of the energy depending on u only, and the set of admissible functions is chosen as  $SBV(\Omega)$ , the space of functions of bounded variation u for which the measure Ducan be written as  $Du = \nabla u\lambda + (u^+ - u^-)n\mathcal{H}^{d-1}|S(u)$ . I. e., the Cantor part of the support of the singular part of the measure known from BV functions, is empty [3]. Here,  $u^+$ and  $u^-$  denote the approximate lim sup resp. liminf of u. The edge set  $\Gamma$  is now represented by  $S_u$  the complement set of Lebesgue points of u, i. e. the measure theoretic discontinuity set of u. Using the compactness of  $SBV(\Omega)$  (cf. AMBRO-SIO, PALLARA, FUSCO [3,40]) and corresponding lowersemicontinuity results, one proves under mild assumptions that there exists a solution  $u \in SBV(\Omega)$  with  $\mathscr{H}^{n-1}(S_u) < \infty$ . Especially due to the complexity of discretizing the singularity set, various approximations  $E_{\varepsilon}$  of the Mumford-Shah functional have been introduced for which  $\Gamma$ -convergence results are known (cf. e. g. [4,5,8,66]). We also refer to [1,71,27,29,43,13] for related topics and further extensions based on the Mumford-Shah functional.

Now, given different images with non aligned edges we can formulate a Mumford Shah type approach for both images with the constraint that the edge set in one images is given as the deformed edge set of the other image, where the deformation is controlled by an additional non linear elastic energy. To ensure that this deformation is one-to-one we consider a polyconvex elastic functional (cf. the work of Ball [6] and the overview given in [24, 30]):

$$E_{\text{reg}}[\phi] = \int_{\Omega} \hat{W}(D\phi, \text{Cof} D\phi, \det D\phi) \,\mathrm{dx}$$
(2)

where  $\hat{W}$  is convex and  $\hat{W} \to \infty$  for det  $D\phi \to 0, +\infty$ .

This overall concept has been worked out in [37] for a level set formulation and in the thesis of one of the authors [36], where in addition to the level set formulation the phase field approach is already presented. In [38] the phase field model for edge registration is combined with the morphological matching approach - first presented in [39] - to achieve a matching of the regular as well as singular image morphologies. In this paper, our focus is on the comparison of the level set and the phase field approach for the simultaneous segmentation and matching of edge sets.

Let us point out, that the free discontinuity based approach proposed here is only a template study which fits into the general formulation of the joint feature extraction and registration problem. Different classes of images may require different models to drive the contour  $\Gamma$  towards the significant features of the images, e. g. a geodesic active contour model as proposed by CASELLES, KIMMEL AND SAPIRO [19]. YEZZI, ZÖLLEI AND KAPUR [52]. have shown results for the coupling of the geodesic contour model and registration. (see also the related work on subjective surfaces by MIKULA, SARTI & SGALLARI [56]) which would lead to a coupled energy of the form

$$E_{\rm ac}[\Gamma,\phi] = \int_{\Gamma} g_R \,\mathrm{d}a + \nu \int_{\Omega} g_R dx + \int_{\Gamma\phi} g_T \,\mathrm{d}a + \nu \int_{\Omega} g_T dx, \quad (3)$$

where  $g_R$  and  $g_T$  correspond to some suitable edge detectors in the images  $u_R$  and  $u_T$ . A common choice is, for example,  $g_u(x) = (1 + s |\nabla u(x)|^2)^{-1}$ , s > 0 (see [48] for a Newton-Type algorithm of the geodesic contour model). A related algorithm is described by UNAL ET AL. [72], taking into account a joint energy for contour curves in different images. FÉRON AND MOHAMMAD-DJAFARI [42] proposed a Bayesian approach for the joint segmentation and fusion of images via a coupling of suitable hidden Markov Models for multi modal images. VEMURI ET AL. have used a level set technique to exploit a reference segmentation in an atlas [73]. We refer to [32] for further ideas.

# 2 A coupled Mumford-Shah model

Minimizing the Mumford-Shah functional we will obtain an approximation of the discontinuity sets of a noisy initial image  $u_0$ , usually supposed to be in  $L^2$ . Now, we consider a template image  $u_T$  and a reference image  $u_R$  at the same

time. Furthermore, we ask for a deformation  $\phi$ , which ensures that the discontinuity set  $S[u_{R,0}]$  will be mapped onto the discontinuity set of  $u_T$ , i. e.,  $\phi(S[u_{R,0}]) = S[u_{T,0}]$ . This can be achieved considered the following functional [37]:

$$\begin{split} \bar{E}_{\mathrm{MS}}[\Gamma,\phi,u_{R},u_{T}] &= \\ \frac{1}{2} \int_{\Omega} (u_{R}-u_{R,0})^{2} \,\mathrm{dx} + \frac{\mu}{2} \int_{\Omega \setminus \Gamma} \|\nabla u_{R}\|^{2} \,\mathrm{dx} + \nu \mathscr{H}^{d-1}(\Gamma) \\ &+ \frac{1}{2} \int_{\Omega} (u_{T}-u_{T,0})^{2} \,\mathrm{dx} + \frac{\mu}{2} \int_{\Omega \setminus \Gamma^{\phi}} \|\nabla u_{T}\|^{2} \,\mathrm{dx} + \nu \mathscr{H}^{d-1}(\Gamma^{\phi}). \end{split}$$

Here  $\Omega \subset \mathbb{R}^d$  is the domain of definition of the images with  $d = 2, 3, u_{T,0}, u_{R,0} \in L^{\infty}(\Omega)$  are the given initial template and reference images,  $\Gamma \subset \Omega$  is (an approximation of) the edge set of the given image  $u_{R,0}$  and  $\Gamma^{\phi} = \phi(\Gamma)$  is the transformed edge-set  $\Gamma$  under the transformation  $\phi$ .

The first line in the integral represents the usual Mumford-Shah segmentation model for the reference image  $u_{R,0}$ , while the second line adapts the same model for the template image  $u_{T,0}$ , but with an edge set given as the image of the edge set in the reference image under the deformation  $\phi$ . Clearly, if  $u_T$  and  $u_R$  are minimizers of the original Mumford-Shah functional and  $\phi$  is chosen such that  $\Gamma^{\phi} = S(u_T)$  this energy is minimal. We see, that the deformation is obviously not uniquely determined by this condition, not even on the edge set itself, since reparametrization along the edge set does not change the energy. Furthermore, the energy does not consider the behavior of  $\phi$  away from the edge set. As proposed above, we add the nonlinear elastic energy  $\alpha E_{reg}[\phi]$ (2), which is supposed to control the regularity of the deformation  $\phi$  and suitably extends deformations onto  $\Omega \setminus \Gamma$ . In order to avoid technical difficulties we avoid the lengthmeasurement of  $\Gamma^{\phi}$  and solely measure the length of  $\Gamma$ . Thus, length of  $\Gamma^{\phi}$  is only implicitly controlled by the length of  $\Gamma$  and the regularity of  $\phi$ . Finally, we end up with the following variational model

$$E[\Gamma, \phi, u_R, u_T] = E_{MS}[\Gamma, \phi, u_R, u_T] + \alpha E_{reg}[\phi], \qquad (4)$$

where

$$E_{\rm MS}[\Gamma, \phi, u_R, u_T] = \frac{1}{2} \int_{\Omega} (u_R - u_{R,0})^2 \, \mathrm{dx} + \frac{\mu}{2} \int_{\Omega \setminus \Gamma} \|\nabla u_R\|^2 \, \mathrm{dx} + \nu \mathscr{H}^{d-1}(\Gamma).$$
$$+ \frac{1}{2} \int_{\Omega} (u_T - u_{T,0})^2 \, \mathrm{dx} + \frac{\mu}{2} \int_{\Omega \setminus \Gamma^{\phi}} \|\nabla u_T\|^2 \, \mathrm{dx}.$$
(5)

# **3** A Level set method

In this section we will review a level set model for the coupled free discontinuity problem (4). Thereby, we restrict ourselves to edge sets which are the union of finitely many Jordan-curves. In this case, the feature set can be viewed as the boundary of detected segments, which are mapped to similar segment boundaries in the second image. For a large class of images, this is a very suitable and convenient approach, since images can often be decomposed into a finite set of independent objects. However this is not always the case. Crack tips might occur not only due to weak edge information but due to the fact that the image contains disrupted discontinuity sets (cf. the phase field approximation below).

In a shape optimization framework [14, 15], we start with an initial shape describing the edge set and evolve it based on a suitable energy descent. The edge set may be elegantly described and propagated by the level set approach of OS-HER and SETHIAN [64, 65]. In [49] a level set based Newton-Type regularized optimization algorithm has been derived for the minimization the original Mumford-Shah functional. That work is the algorithmical basis for our method. For related approaches we refer to [23,21,22,49]. In explicit, we consider  $\Gamma$  to be given as the zero level set of the level set function  $v_{\Gamma} : \Omega \to \mathbb{R}$ , i. e.,

$$\Gamma = \left\{ x : v_{\Gamma}(x) = 0 \right\}.$$

# 3.1 The reduced functional

The functional (4) depends on the variables  $u_R$ ,  $u_T$ ,  $\phi$  and  $\Gamma$ . In the process of minimization we may devise different strategies for the different variables. Fortunately the functional is quadratic in the variables  $u_R$  and  $u_T$ . Hence, we may minimize the energy for fixed  $\Gamma$  and  $\phi$  over image spaces of  $u_R$  and  $u_T$ . Let us now denote by  $u_R[\Gamma]$  and  $u_T[\Gamma, \phi]$  the corresponding minimizers. They are obtained solving the Euler Lagrange equations with respect to  $u_R$  and  $u_T$ :

$$-\mu\Delta u_{R} + u_{R} = u_{R,0} \quad \text{in } \Omega \setminus \Gamma$$
  

$$\partial_{n_{\Gamma}} u_{R} = 0 \quad \text{on } \Gamma^{\phi}$$
  

$$-\mu\Delta u_{T} + u_{T} = u_{T,0} \quad \text{in } \Omega \setminus \Gamma^{\phi},$$
  

$$\partial_{n_{\Gamma}} u_{T} = 0 \quad \text{on } \Gamma.$$
(6)

It is obvious that the minimizer with respect to  $u_R$  depends only on  $\Gamma$ , whereas the minimizer with respect to  $u_T$  depends also on u via the domain of integration  $\Omega \setminus \Gamma^{\phi}$ . Now we can define the *reduced* functional

$$\hat{E}[\Gamma,\phi] = E[\Gamma,\phi,u_R[\Gamma],u_T[\Gamma,\phi]].$$
(7)

To treat the optimization problem in  $\Gamma$  represented by the level set function  $v = v_{\Gamma}$  we make use of nowadays classical shape sensitivity calculus. For details we refer to the books of SOKOŁOWSKI & ZOLÉSIO [69] or DELFOUR & ZOLÉSIO [34]. Furthermore the Appendix of [49] gives a nice overview. For an energy  $E[\Gamma] = \int_{\Gamma} \theta \, da$  depending on a domain boundary  $\Gamma$  we get

$$\langle \partial_{\Gamma} E[\Gamma]; \zeta \rangle = \int_{\Gamma} (\partial_{n_{\Gamma}} \theta + \theta h) \zeta \cdot n_{\Gamma} \, \mathrm{d}a$$
 (8)

where  $\Gamma$  is supposed to be a  $\mathscr{C}^1$ -hypersurface and  $\zeta$  is a scalar perturbation of  $\Gamma$  in normal direction. Furthermore,

for an energy  $E[\Omega] = \int_{\Omega} \theta(\Omega, x) dx$  depending on a domain  $\Omega$  the shape derivative is given by

$$\langle \partial_{\Gamma} E[\Omega]; \zeta \rangle = \int_{\Omega} \theta'(\Omega; \zeta) \,\mathrm{dx} + \int_{\Gamma} \theta \,\zeta \,\mathrm{d}a,$$
 (9)

where  $\theta'(\Omega)$  is the shape derivative of the integrand  $\theta$  with respect to a normal variation  $\zeta$  of the domain boundary  $\Gamma$ extended to the whole domain. For details we refer to [37]. With these tools available, we are now able to derive the first variation of the reduced function  $\hat{E}$  (7) with respect to the shape variable  $\Gamma$  and with respect to the deformation  $\phi$ . Via a integral transform, we first decouple  $\Gamma$  and  $\phi$  and obtain

$$\begin{split} \tilde{E}(\Gamma,\phi) &= \\ \frac{1}{2} \int_{\Omega} (u_R(\Gamma) - u_{R,0})^2 \, \mathrm{dx} + \frac{\mu}{2} \int_{\Omega \setminus \Gamma} \|\nabla u_R(\Gamma)\|^2 \, \mathrm{dx} \\ &+ \frac{1}{2} \int_{\Omega} \left( (u_T(\Gamma,\phi) - u_{T,0})^2 \circ \phi \right) |\det D\phi| \, \mathrm{dx} \\ &+ \frac{\mu}{2} \int_{\Omega \setminus \Gamma} \left( \|\nabla u_T(\Gamma,\phi)\|^2 \circ \phi \right) |\det D\phi| \, \mathrm{dx} \\ &+ v \mathscr{H}^{d-1}(\Gamma) + \alpha E_{\mathrm{reg}}[\phi] \end{split}$$

Now we can apply (8) as well as (9), where we have to integrate along the boundaries from both sides of the contour, which leads to corresponding jump terms. We obtain

$$\begin{split} \left\langle \partial_{\Gamma} \hat{E}[\Gamma,\phi];\zeta\right\rangle &= \\ \frac{1}{2} \int_{\Gamma} \left( \left[ \left( u_{R}(\Gamma) - u_{R,0}\right)^{2} \right] + \mu \left[ \left\| \nabla u_{R}(\Gamma) \right\|^{2} \right] \right) \zeta \,\mathrm{d}a \\ &+ \frac{1}{2} \int_{\Gamma} \left( \left[ \left( u_{T}(\Gamma,\phi) - u_{T,0}\right)^{2} \right] \\ &+ \mu \left[ \left\| \nabla u_{T}(\Gamma,\phi) \right\|^{2} \right] \right) \circ \phi \left| \det D\phi \right| \zeta \,\mathrm{d}a \\ &+ v \int_{\Gamma} h \zeta \,\mathrm{d}a. \end{split}$$
(10)

Recall that  $u_R[\Gamma]$  and  $u_T[\Gamma, \phi]$  are defined as the solutions of the corresponding elliptic boundary value problems (6). As described in [49], the terms involving the shape derivatives  $\theta'$  disappear since they are derivatives of the energy w.r.t.  $u_R$  and  $u_T$  in direction of  $u'_R$  resp.  $u'_T$  and hence zero due to local optimality.

For Frèchet derivative of  $\hat{E}$  with respect to the deformation  $\phi$  in a direction  $\psi$  we obtain

$$\begin{split} \langle \partial_{\phi} \hat{E}[\phi]; \psi \rangle &= \frac{1}{2} \int_{\Gamma^{\phi}} \left( \llbracket |u_{T}(\Gamma, \phi) - u_{T,0}|^{2} \rrbracket \right. \\ &+ \mu \llbracket |\nabla u_{T}(\Gamma, \phi)|^{2} \rrbracket \right) (\psi \circ \phi^{-1} \cdot n_{\Gamma^{\phi}}) \, \mathrm{d}a \\ &+ \left\langle \partial_{\phi} E_{\mathrm{reg}}[\phi]; \psi \right\rangle, \quad (11) \end{split}$$

where the transformed normal  $n_{\Gamma\phi}$  is given by

$$n_{\Gamma^{\phi}} = \frac{\operatorname{Cof} D\phi n_{\Gamma}}{\|\operatorname{Cof} D\phi n_{\Gamma}\|}.$$

# 3.2 Regularized gradient descent

The first variations contain jump terms of  $u_T - u_{T,0}$  resp.  $u_R - u_{R,0}$ , for in general noisy initial data  $u_{R,0}$  and  $u_{T,0}$ . Hence the regularity of the descent direction with respect to the  $L^2$  metric is expected to be low. Thus, we will incorporate a regularized gradient descent (cf. [25,26]) with respect to both variables of the reduced functional  $\hat{E}$ .

As a metric on the space of deformation  $\phi$  we consider

$$g^{\sigma}_{\phi}(\psi,\xi) = \int_{\Omega} \psi \cdot \xi + \frac{\sigma^2}{2} \nabla \psi : \nabla \xi \,,$$

where  $A : B = tr(A^T B)$ . Let us remark that the inverse of the corresponding metric tensor is related to a Gaussian filtering of the deformation with filter width  $\sigma$ . Thus, the regularized descent direction  $\psi[\Gamma, \phi]$  is given as a solution of the elliptic problem

$$g^{\sigma}_{\phi}(\psi[\Gamma,\phi],\xi) = -\left\langle \partial_{\phi}\hat{E}[\Gamma,\phi];\xi \right\rangle \tag{12}$$

for all variations  $\psi$  of  $\phi$ .

Next, we discuss the regularization of the shape gradient with respect to the geometric variable  $\Gamma$ . We aim at finding a metric on normal variations of  $\Gamma$ , such that this resulting regularization is balanced with the regularized descent in the deformation. Hence, we ask for a suitable metric  $g_{\Gamma}^{\sigma}$  and defined a normal variation  $\zeta[\Gamma, \phi]$  on  $\Gamma$  as the regularized descent direction with respect to  $\Gamma$  by

$$g_{\Gamma}(\zeta[\Gamma,\phi],\theta) = -\langle \partial_{\Gamma} \hat{E}[\Gamma,\phi];\theta\rangle$$
(13)

An  $H^{1,2}$  regular descent direction  $d[\Gamma, \phi]$  as we obtain it above, induces a motion of the transformed edge set  $\Gamma^{\phi}$  with a speed in normal direction which is given by  $d \circ \phi^{-1} n_{\Gamma^{\phi}} \in$  $H^{\frac{1}{2}}(\Gamma^{\phi})$  for  $\Gamma^{\phi}$  sufficiently regular. This motivates us to choose the shape gradient with respect to a suitable  $H^{\frac{1}{2}}$ metric on  $\Gamma$ . By this choice we expect a reasonable balance between the regularization of update directions for the functional variable  $\phi$  and the geometric variable  $\Gamma$ . In order to define an inner product on  $H^{\frac{1}{2}}(\Gamma)$  let us consider the boundary value problem

$$-\frac{\sigma^2}{2}\Delta\zeta + \zeta = 0 \text{ in } \Omega,$$
  
$$\partial_{n_{\Gamma}}\zeta = \eta \text{ on } \Gamma,$$
 (14)

for a some functional  $\eta \in H^{-\frac{1}{2}}(\Gamma)$  given on  $\Gamma$ . Let us denote by  $\mathscr{N}: H^{-\frac{1}{2}}(\Gamma) \to H^{\frac{1}{2}}(\Gamma)$  the linear operator representing the *Neumann-to-Dirichlet map* which maps w in (14) to the Dirichlet trace  $\zeta|_{\Gamma}$  of the solution to (14). It is well known (cf.[54]) that  $\mathscr{N}$  is an isomorphism. Finally, we define

$$g^{\sigma}_{\Gamma}(\zeta,\theta) := \left\langle \mathscr{N}^{-1}\zeta; \theta \right\rangle_{H^{-\frac{1}{2}}(\Gamma) \times H^{\frac{1}{2}}(\Gamma)}$$

Thus, to evaluate the regularized shape gradient, we have to solve (14) with  $\eta = \partial_{\Gamma} \hat{E}$  and to evaluate the trace of the solution on  $\Gamma$ .

# 3.3 A level set shape gradient descent method

In what follows let us describe how the optimization, that takes place over a shape and the deformation simultaneously, can be performed algorithmically. The topology of the solution  $\Gamma$  of the optimization problem is not known *a-priori*. On the other hand, the gradient descent method depends on an initial guess. Level set methods provide a convenient framework for the representation and numerical evolution of sharp interfaces, especially when topological changes come into play. A detailed description of the finite element algorithm can be found in [37]. Here, we only briefly describe the key components in each step of the gradient descent:

• For given discrete deformation  $\phi$  and level set function v the finite element solution for  $u_R$  and  $u_T$  in (6) on both sides of the interface is computed independently applying a Composite Finite Elements (cf. [46,67,75]). Thus, we avoid an explicit remeshing of the domains separated by the current level set of v representing the edge set  $\Gamma$ . Furthermore, it allows for an efficient multigrid solution of these elliptic problems, which leads leads to a significant speed-up of the algorithm. The transformation vector field  $\phi$  is discretized using standard Finite Elements.

• Once finite element approximations of  $u_R$  and  $u_T$  are known, the shape gradient and the gradient with respect to the deformation can be computed as finite element approximation on the domain  $\Omega$  described by (13) and (12). Again two linear elliptic problems have to be solved to evaluate these regularized gradients.

• The gradient descent step in the deformation variable  $\phi$  is performed in a straightforward way.

• To evolve the level set function with a speed on the contour given by the discrete  $\zeta[\Gamma, \phi]$  on the discrete level set  $\Gamma$ , we consider an extension  $\tilde{\zeta}$  onto a small neighborhood of the contour. Here, we have the widely used approach based on the solution of the transport equation

$$\nabla \tilde{\zeta} \cdot \nabla d_{\Gamma} = 0$$
 on  $\Omega$  and  $\tilde{\zeta} = \zeta [\Gamma, \phi]$  on  $\Gamma$ ,

where  $d_{\Gamma}$  represents the signed distance function with respect to  $\Gamma$  (cf. [63,68]). We used the method proposed by BORNEMANN & RASCH [9].

• For the actual evolution of the level set function *v* via

$$\partial_t v + \tilde{\zeta} \|\nabla v\| = 0 \quad \text{on} \quad \Omega$$
 (15)

we have applied a third-order accurate ENO-scheme (cf. [63]).

## 3.4 Numerical experiments

In Figure 1 we have applied the algorithm to a pair of brain images. The top row shows a *proton density* weighted MR scan, while the bottom row shows a T1-weighted magnetic resonance image of the same patient. The initial misfit consists mainly of a shift and a small rotation. The algorithm finds the brain structure in both images well after about 250 steps, and the resulting deformation consists mainly of a shift enhanced by some minor local deformations.



**Fig. 1** Matching with the sharp interface Mumford-Shah model. TOP ROW: Reference image  $u_R$  (proton density weighted MR-image (PD) of a human brain) an  $u_T$  (T1-weighted MR-image). MIDDLE ROW: Deformation plot and the matching result  $u_T \circ \phi$ . BOTTOM ROW: Initial misfit shown as an striped overlaid reference and template compared to the final matching result. The parameters were chosen as  $\mu = 200$ ,  $\nu = 250$  and  $\alpha = 5000$ . The iteration converged after 250 iterations.

Figure 3 demonstrates the competing effect of the regularization and the energy contributions which pull the contour towards the edges. We can exploit this in order to map an original reference shape (top row) to a given object, where the shape is partially corrupted (bottom row). Apart from the destroyed region the shapes differ also by a non-rigid deformation plus a translation. This can be well observed in the second column. At this stage, the regularization dominates and prohibits the contour in the bottom row to evolve towards the "visible" edge and prefers to adopt the contour from the reference image. This yields a reconstruction of the destroyed shape, which is optimal with respect to the regularization energy.

Fig. 3 Towards model-based reconstruction. The image at the TOP LEFT shows an artificial reference model of a tooth. On the BOTTOM LEFT a nonlinearly deformed version of the reference with a large destroyed region is shown. Both images also show the initial contour  $\Gamma$ . The sequence shows the evolution of  $\Gamma$  and  $\Gamma^{\phi}$  for the iteration numbers 0, 20, 80, 320, where the parameters were chosen as  $\mu = 50$ ,  $\alpha = 200 \text{ and } v = 5000.$ 

the Mumford-Shah energy [31, 61, 5, 12, 2] to

$$F[u] = \frac{1}{2} \int_{\Omega} (u - u_0)^2 \,\mathrm{d}\mathbf{x} + \frac{\mu}{2} \int_{\Omega \setminus \Gamma} \|\nabla u\|^2 \,\mathrm{d}\mathbf{x} + \mathbf{v} \mathscr{H}^{d-1}(S_u)$$

on the space of piecewise  $\mathscr{C}^1$  functions

$$PC^{1}(\Omega) = \left\{ u \in L^{\infty}(\Omega) \right\} \left\{ u \in \mathscr{C}^{1}(\Omega \setminus \overline{S_{u}}) \\ \text{and } \mathscr{H}^{d-1}(\overline{S_{u}} \cap \Omega \setminus S_{u}) = 0 \right\}.$$
(16)

Here,  $S_u$  denotes the complement of the set of Lebesgue points of u. Since  $PC^1$  is not compact with respect to a suitable topology, the common approach is to relax F to

$$\overline{F}(u) = \inf\left\{\liminf_{s\to\infty} F(u_s) : u_s \to u \in L^2(\Omega), u_s \in PC^1(\Omega)\right\}.$$

The approximation proposed by AMBROSIO&TORTORELLI in [5] results from a minimization of the functional

$$E_{\varepsilon}[u,v] = \int_{\Omega} \left\{ \frac{1}{2} (u-u_0)^2 + \frac{\mu}{2} (v^2 + k_{\varepsilon}) \|\nabla u\|^2 \right\} dx$$
$$+ v \int_{\Omega} \left\{ \varepsilon \|\nabla v\|^2 + \frac{(1-v)^2}{4\varepsilon} \right\} dx$$

for fixed  $\varepsilon$  and  $k_{\varepsilon} > 0$ . Here, *v* is a phase field variable which is supposed to be approximately 1 apart from the interface and approximate 0 on the edge set with a transition region of width  $2\varepsilon$ . They have shown the  $\Gamma$ -convergence of  $E_{\varepsilon}$ to the functional defined by  $\overline{E}[u,v] = \overline{F}[u]$ , iff  $v \equiv 1$ , and  $\overline{E}[u,v] = +\infty$  otherwise. The  $\Gamma$ -convergence is respect with to the strong  $L^2$  topology.

Now, we suggest for the joint segmentation and registration problem an analogous coupled phase-field formulation by again introducing an auxiliary phase field variable v, describing the singularity set  $S_T$  of the image  $u_T$ , but at the



Now, let us present an alternative to the previously described sharp interface model. In [5] Ambrosio and Tortorelli proposed a phase field approximation of the Mumford-Shah [62] functional (1). Before we revise the approximation, we rewrite same time  $v \circ \phi$  should energetically describe the edge set

Fig. 2 Evolution of  $\Gamma$  in  $u_R$  in the left column and the evolution of  $\phi(\overline{\Gamma})$  in  $u_T$  in the right column for iteration numbers 0, 50, 150 and

250 for the images and the problem setup as in Figure 1.



 $S_R$  in the image  $u_R$ . A corresponding energy formulation is then given by the minimization of

$$E_{AT}^{\varepsilon}[u_{R}, u_{T}, v, \phi] := \frac{1}{2} \int_{\Omega} \left\{ (u_{R} - u_{R,0})^{2} + (u_{T} - u_{T,0})^{2} \right\} dx + \frac{\mu}{2} \int_{\Omega} \left\{ (v^{2} \circ \phi + k_{\varepsilon}) \| \nabla u_{R} \|^{2} + (v^{2} + k_{\varepsilon}) \| \nabla u_{T} \|^{2} \right\} dx + \frac{\nu}{2} \int_{\Omega} \left\{ \varepsilon \| \nabla v \|^{2} + \frac{1}{4\varepsilon} (v - 1)^{2} \right\} dx$$
(17)

with  $k_{\varepsilon} = o(\varepsilon)$ . Here, the phase field function *v* corresponds to the contour  $\Gamma^{\phi}$  and the contour  $\Gamma$  is described by  $v \circ \phi$ . The first integral measures the deviation of  $u_R$  and  $u_T$  to the data in the  $L^2$ -sense. The second integral now forces the signature  $v^2$  to be small where  $u_T$  has steep gradients and, correspondingly,  $v^2 \circ \phi$  to be small where  $u_R$  has steep gradients. On the other hand, this determines  $\phi$  to align the signature function in the reference domain to line up with the edges of  $u_R$ , and finally, for fixed signature and deformation, the smoothness of the images  $u_R$  and  $u_T$  is controlled, i. e., steep gradients of  $u_T$  are penalized where  $v \not\approx 0$  and analogously for  $u_R$ .

Again, the deformation  $\phi$  will mainly be determined along the discontinuity sets. Indeed, as outlined above, away from the contours the phase field v will approximately be identical to 1, and hence variations of  $\phi$  will not change the energy in these regions. Hence, we again consider a nonlinear hyperelastic regularization given by the additional energy function  $E_{reg}[\phi]$  (2) and finally define

$$E^{\varepsilon}[u_R, u_T, v, \phi] = := E^{\varepsilon}_{AT}[u_R, u_T, v, \phi] + \alpha E_{reg}[\phi]$$

. .

and ask for minimizers.

In contrast to the original approach of [4], where approximating elliptic but non-quadratic functionals have been used, the approximation of (17) gives rise to practicable numerical methodologies. We refer for instance to [7,66]. In order to discretize  $E_{\text{ATreg},\varepsilon}$ , we follow the approach of BOUR-DIN. In [10] he has proven the  $\Gamma$ -convergence of the discretized functionals against the functional  $\overline{E}$ . See also (cf. [11,41,20,35]).



Fig. 4 Matching and results of the same problem set-up as in Figure 1. TOP ROW: Initial images  $u_R$  (PD) and  $u_T$  (T1). MIDDLE ROW: Deformation plot and matching results  $u_T \circ \phi$ . BOTTOM ROW: comparison of initial misfit and final matching result against the reference image.



Fig. 5 Comparison of the phase-field function v after the first iteration (LEFT) and after the final iteration (RIGHT)

# 4.1 First variation of the energy

Let us first calculate the variations with respect to the variables  $u_R$ ,  $u_T$  and v in directions  $\vartheta$ ,  $\xi$ , and  $\zeta$ , respectively:

$$\langle \partial_{u_R} E_{AT}^{\varepsilon} [u_R, u_T, v, \phi]; \vartheta \rangle = \int_{\Omega} (u_R - u_{R,0}) \cdot \vartheta \, \mathrm{dx} + \mu \int_{\Omega} (v^2 \circ \phi + k_{\varepsilon}) \nabla u_R \cdot \nabla \vartheta \, \mathrm{dx} \langle \partial_{u_T} E_{AT}^{\varepsilon} [u_R, u_T, v, \phi]; \xi \rangle = \int_{\Omega} (u_T - u_{T,0}) \cdot \xi \, \mathrm{dx} + \mu \int_{\Omega} (v^2 + k_{\varepsilon}) \nabla u_T \cdot \nabla \xi \, \mathrm{dx} \langle \partial_v E_{AT}^{\varepsilon} [u_R, u_T, v, \phi]; \zeta \rangle = \mu \int_{\Omega} \| \nabla u_T \|^2 v \cdot \zeta \, \mathrm{dx} + \mu \int_{\Omega} \| \nabla u_R \|^2 (v \circ \phi) \cdot (\zeta \circ \phi) + v \int_{\Omega} \varepsilon \nabla v \cdot \nabla \zeta \, \mathrm{dx} + v \int_{\Omega} \frac{1}{4\varepsilon} (v - 1) \zeta \, \mathrm{dx} .$$
(18)

We rewrite (18) via the transformation formula:

$$\langle \partial_{\nu} E_{AT}^{\varepsilon} [u_{R}, u_{T}, \nu, \phi]; \zeta \rangle = \mu \int_{\Omega} \|\nabla u_{T}\|^{2} \nu \cdot \zeta \, \mathrm{dx}$$

$$+ \mu \int_{\Omega} \|\nabla u_{R}\|^{2} \circ \phi^{-1} \nu \cdot \zeta \, \mathrm{det} \, D\phi^{-1} \, \mathrm{dx}$$

$$+ \nu \int_{\Omega} \varepsilon \nabla \nu \cdot \nabla \zeta \, \mathrm{dx} + \nu \int_{\Omega} \frac{1}{4\varepsilon} (\nu - 1) \zeta \, \mathrm{dx}.$$
 (19)

Hence, for fixed v and  $\phi$  the reconstructed images  $u_R$  and  $u_T$  can be computed by solving the following elliptic problems

$$u_{R} - \mu \operatorname{div} \left( (v^{2} \circ \phi + k_{\varepsilon}) \nabla u_{R} \right) = \mathscr{I}_{h} u_{R,0,\varepsilon} \quad \text{in } \Omega,$$
  
$$\partial_{v} u_{R} = 0 \quad \text{on } \partial \Omega \qquad (20)$$

$$u_T - \mu \operatorname{div} \left( (v^2 + k_{\varepsilon}) \nabla u_T \right) = \mathscr{I}_h u_{T,0,\varepsilon} \quad \text{in } \Omega,$$
  
$$\partial_v u_T = 0 \quad \text{on } \partial \Omega.$$
(21)

Since  $v \ge 0$  the corresponding bilinear-forms are coercive. Furthermore, we are able to find for each  $u_T$ ,  $u_R$  and  $\phi$  the optimal phase field v as the solution of the Euler-Lagrange equation with respect to the variation in the variable v, i. e.,

$$\mu \|\nabla u_T\|^2 v + \mu \|\nabla u_R\|^2 \circ \phi^{-1} v \det D\phi^{-1} + \frac{v}{4\varepsilon} (v-1) - v\varepsilon \Delta v = 0 \qquad \text{in } \Omega. \quad (22)$$

and  $\partial_v v = 0$  on  $\partial \Omega$ . Finally, the variation of the energy with respect to the deformation in a direction  $\psi$  is given by

$$\begin{split} \left\langle \partial_{\phi} E_{AT}^{\varepsilon} [u_{R}, u_{T}, v, \phi]; \psi \right\rangle &= \\ \mu \int_{\Omega} \|\nabla u_{R}\|^{2} v \circ \phi \left( \nabla v \circ \phi \cdot \psi \right) dx \\ &= \mu \int_{\Omega} \|\nabla u_{R}\|^{2} \circ \phi^{-1} v \left( \nabla v \cdot \psi \circ \phi^{-1} \right) \det D \phi^{-1} dx \,. \end{split}$$

$$(23)$$

Analogously to the approach chosen in the above sharp interface model, the energy functional can be reduced to depending only on  $\phi$ , where  $u_R[\phi]$ ,  $u_T[\phi]$  and  $v[\phi]$  are determined as the unique solutions to the quadratic minimization problem for fixed  $\phi$ :

$$\hat{E}^{\varepsilon}[\phi] = E^{\varepsilon}[u_R[\phi], u_T[\phi], v[\phi], \phi].$$
(24)

# 4.2 Multiscale gradient descent

Different to the sharp interface approach above the phase field approximation comes along with a natural scale parameter. As mentioned above the width of the diffusive interface turns out to be  $2\varepsilon$ . On the same scale the images  $u_T$  and  $u_R$  are diffused close to edges of the initial images  $u_{T,0}$  and  $u_{R,0}$ . Hence, the smoothness of energy variations will also depend on the scale parameter  $\varepsilon$ . On coarser scales we expect smoother descend directions and larger displacement can be rendered via the gradient descent. But, for decreasing  $\varepsilon$  one observed successively irregular variations. Indeed, the smoothness of  $\partial_{\phi} E_{AT}^{\varepsilon}$  is controlled by the smoothness of  $\phi^{-1}$ ,  $u_R$  and v and the smoothness of v is steered directly by  $\varepsilon$  on account of the penalty term  $\varepsilon \|\nabla v\|^2$ . Furthermore, for a small  $\varepsilon$ , *v* is close to 0 where  $\|\nabla u_R\|^2 \circ \phi^{-1}$  or  $\|\nabla u_T\|^2$  are large and v is forced to be close to 1 in the rest of the domain on account of the amplified single well potential.

In summary, larger values of  $\varepsilon$  yield coarse and smooth approximations of the images, the phase field and the deformation. Hence, one starts with coarse approximations, to find a stationary point in the simplified energy landscape, iteratively reduces the approximation parameter  $\varepsilon$  by taking the solution of the previous scale as the new initial guess on the next finer scale.

Then on finer scales for small values of  $\varepsilon$ , the discrete descent direction tend to get irregular. Hence, it is again feasible to consider a regularized gradient descent and we consider the same regularized metric on variations of the deformation as in the sharp interface case.

On each scale the resulting finite element algorithm consists of a discrete gradient descent. Each gradient descent step can be decomposed as follows. For given  $\phi$  compute Composite Finite Element approximations for  $u_T$ ,  $u_R$  and v as discrete solutions of (20), (21), and (22), respectively. Iterate these three solutions steps until convergence. Then evaluate the descent direction in the deformation taking into account Finally, perform an update of the deformation  $\phi$ based on a line-search strategy.

Let us remark that on the finest scale  $\varepsilon$  has to be of the order of the grid size. Otherwise the transition zone cannot be resolved by a Finite Element function.

#### 4.3 Numerical experiments

In Figure 4, we test the phase field algorithm with the same data as in the case of the sharp interface model. We observe very similar results. In fact, the phase field model seems to perform a better alignment in the interior of the skull. The phase field function captures edge details in the entire image, while the sharp interface framework focuses on the evolution of the predefined contour. This leads to a positive effect on the final alignment and to a slightly improved deformation. This can be seen very clearly in Figure 5. It shows the phase field function at the initial stage and the final stage. Since, the coupled discontinuity problems aims at keeping the length of the interface short, the deformation will eventually try to map the edges in  $u_R$  onto the edges of  $u_T$ .

## 5 The main differences between the two approaches

The aim of this comparison of the level set and the phase field model is to illustrate and discuss the drawbacks and benefits of both approaches in this particular application of joint segmentation and registration. It naturally depends on the computational considerations, the conceptual framework and the specific application, which alternative will be the method of choice. In the following we will point out some fundamental differences.

## 5.1 Methodological differences

Both, the level set approach and the phase field approach are famous for their topological flexibility. The process of splitting a curve into several curves is a smooth process in both frameworks and does not cause any conceptual problems.

The representations of the discontinuity set are fundamentally different in type. The level set method elegantly allows to represent, trace and evolve a given sharp interface. This fits well to the framework of the calculus of shape derivatives in which the current interface is given precisely. To be more precise, the level set method is just one way of evolving a sharp interface, in comparison to parametrizing the interface. We consider parametric versions as not competitive due to tremendous difficulties that arise at topology changes. For the sake of completeness, let us mention that one can also describe sharp interfaces by a phase field function by using suitable obstacle potentials. From the conceptional viewpoint of shape variation, those would then fall in the same category, since the motion would result from the shape variation of the shape functional. The AMBROSIO-TORTORELLI-approximation is however a diffuse representation. Instead of precisely representing the position of the interface, the phase-field function v only indicates the position of edges in a blurry way. This phase-field function has to be defined on the entire domain  $\Omega$  and results directly from the solution of a simple elliptic PDE. The actual discontinuity set is then only given as minimizer  $\Omega \to \{0,1\}$ of the  $\Gamma$ -limit of sequence of approximation functionals for  $\varepsilon \rightarrow 0$ . In actual computations however the phase field function has to be computed for  $\varepsilon$  of the order of the grid size. We conclude, that if the actual interface is of interest as the result of the algorithm, a sharp interface model, represented e. g. by a level set function is favorable.

The classical level set framework is restricted to closed curves, and thus it does not allow to represent crack tips by a single level set function. Although this could be achieved by combining several level set functions with boolean operations, the phase field approach appears to be more flexible and practicable for the applications discussed here. The same is true for generating holes. The phase field representation is global by definition and respects the features of the images in the entire domain, with requiring any initialization. For sharp interface models, let us mention the concept of topological derivatives [16]. By considering the limit for the change of the energy functional for arbitrary small holes, one can yield a descent of the functional with respect to topology. This is of great importance for example in structural mechanics. The sharp interface approach optimizes with respect to a given initial shape, while the phase field approach will try to align all dominant edges in the images simultaneously. In some cases however, when there are no counterparts of strong edges in the other image, the simultaneous matching of all features may be a counterproductive aim. The restriction to certain features only may be beneficial here.

The dependence on the initial condition in the case of the sharp interface model, does not necessarily mean to be a burden. Due to the non-convex structure of the joint discontinuity problem, the initial shape and position of the contour allows to give the user some kind of control over the matching process.

#### 5.2 Computational considerations

Let us now compare the algorithmical effort related to both of the approaches. The phase field method can be set up in a straightforward way by solving elliptic and parabolic problems with coefficients which vary in space. Such problems are standard and can be solved with all PDE toolboxes. Due to the fact that the interface is represented by a smooth phase field function, the solution of the Helmholtz problems in the domains, which are divided by the free discontinuity is straightforward and does not require any additional effort to take care about free boundaries.

The sharp interface approach is more complicated to implement. The computation of the velocity requires to evaluate geometric entities and jumps of the traces of the functions  $u_R$  and  $u_T$  along the interface. In order to compute these functions, an algorithmical tool like Composite Finite Elements, a *Shortley-Weller* discretization or *Websplines* [50] has to be incorporated. In order to improve efficiency multigrid methods [45] have been applied. All this effort is honored by yielding the true derivative and thus the correct dynamics of the gradient flow. However, for the task of image registration, we are mainly interested in the minimization of the functional and not the evolution of the contour.

## 6 Conclusion

We have compared a level set based and a phase field model for simultaneous segmentation and registration of images by incorporating a Mumford-Shah type energy on the reference image as well as the template image, where the contour is transformed into the template image by a regularized deformation. The work is motivated by the fact, that, given an exact registration of two images of different modality, edge-extraction and segmentation can be enhanced considerably by combining complementary feature information from both modalities. On the other hand the process of registering a pair of images may rely on segmentations and featureextractions of both images, which is often a very tedious process, especially if in some areas the feature information is very weak. Due to the coupling of the edge sets by the smooth deformation, the edge is driven to its correct shape.

Due to the regularization of the gradient flow, the minimization process has turned out to be stable and requires only a small number of iterations until convergence. On the other hand, the regularization and necessity of determining the solutions of the Helmholtz equations in the regions  $\Omega_1$ and  $\Omega_2$  requires the solution of elliptic PDEs.

The phase field method offers an interesting, convenient and efficient alternative to the level set approach if the main aim is registration and not segmentation. In contrast to the level set function, the phase field parameter captures edge information in the entire domain. From an algorithmical point of view, the phase field method is certainly much easier to handle and only requires the solution of standard elliptical problems.

Both methodologies are very flexible and allow a wide range of extensions for model-based matching (introducing *a-priori* knowledge into the functional as e. g. in [27,29]), optical flow estimation with discontinuities (see also [28]) and other areas.

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## References

- Alvarez, L., Snchez, J., Deriche, R., Weickert, J.: Dense disparity map estimation respecting image discontinuities: A pde and scalespace based approach. IAPR Workshop on Machine Vision No. 28-30, 423–427 (2000)
- Ambrosio, L., Faina, L., March, R.: Variational approximation of a second order free discontinuity problem in computer vision. SIAM J. Math. Anal. 32(6), 1171–1197 (2001)
- Ambrosio, L., Fusco, N., Pallara, D.: Functions of bounded variation and free discontinuity problems. Oxford University Press (2000)
- Ambrosio, L., Tortorelli, V.M.: Approximation of functionals depending on jumps by elliptic functionals via Γ-convergence. Comm. Pure Appl. Math. 43, 999–1036 (1990)

- Ambrosio, L., Tortorelli, V.M.: On the approximation of free discontinuity problems. Boll. Un. Mat. Ital. B 6(7), 105–123 (1992)
- Ball, J.: Global invertibility of Sobolev functions and the interpenetration of matter. Proc. Roy. Soc. Edinburgh 88A, 315–328 (1988)
- Belletini, G., Coscia, A.: Discrete approximation of a free discontinuity problem. Num. Funct. Anal. Optim. 15, 201–224 (1994)
- Bonnet, A.: On the regularity of the edge set of Mumford-Shah minimizers. Prog. in Nonlinear Differential Equations and Their Applications 25, 93–103 (1996)
- 9. Bornemann, F., Rasch, C.: Finite-Element discretization of static Hamilton-Jacobi equations based on a local variation principle. to appear in (2004)
- Bourdin, B.: Image segmentation with a Finite Element method. ESIAM: Mathematical Modelling and Numerical Analysis 33(2), 229–244 (1999)
- 11. Bourdin, B., Chambolle, A.: Implementation of a Finite-Element approximation of the Mumford-Shah functional. Numer. Math. **85**(4), 609–646 (2000)
- 12. Braides, A.: Approximation of Free Discontinuity Problems, *Lecture Notes in Mathematics*, vol. 1694. Springer-Verlag (1998)
- Brook, A., Kimmel, R., Sochen, N.A.: Variation restoration and edge detection for color images. J. Math. Imag. and Vis. 18, 247– 268 (2003)
- Burger, M.: A framework for the construction of level set methods for shape optimization and reconstruction. Interfaces and Free Boundaries 5, 301–329 (2003)
- Burger, M.: Levenberg-Marquardt level set methods for inverse obstacle problems. Inverse Problems 20, 259–282 (2004)
- Burger, M., Hackl, B., Ring, W.: Incorporating topological derivatives into level set methods. J. Comp. Phys. **194**, 344–362 (2004)
- Caselles, V., Catté, F., Coll, T., Dibos, F.: A geometric model for active contours in image processing. Numer. Math. 66, 1–31 (1993)
- Caselles, V., Coll, B.: Snakes in movement. SIAM J. Numer. Analy. 33(6), 2445–2456 (1996)
- Caselles, V., Kimmel, R., Sapiro, G.: Geodesic active contours. International Journal of Computer Vision 22(1), 61–79 (1997)
- Chambolle, A.: Image segmentation by variatonal methods: Mumford-Shah functional and the discrete approximations. SIAM J. Appl. Math. 55(3), 827–863 (1995)
- Chan, T.F., Vese, L.A.: Image segmentation using level sets and the piecewise constant Mumford-Shah model. UCLA CAM Report 00-14, University of California, Los Angeles (2000)
- Chan, T.F., Vese, L.A.: A level set algorithm for minimizing the Mumford-Shah functional in image processing. UCLA CAM Report 00-13, University of California , Los Angeles (2000)
- Chan, T.F., Vese, L.A.: Active contours without edges. IEEE Trans. Image Processing 10(2), 266–277 (2001)
- Ciarlet, P.G.: Three-Dimensional Elasticity. Elsevier, New York (1988)
- Clarenz, U., Droske, M., Rumpf, M.: Towards fast non-rigid registration. In: Inverse Problems, Image Analysis and Medical Imaging, AMS Special Session Interaction of Inverse Problems and Image Analysis, vol. 313, pp. 67–84. AMS (2002)
- Clarenz, U., Henn, S., Rumpf M. Witsch, K.: Relations between optimization and gradient flow methods with applications to image registration. In: Proceedings of the 18th GAMM Seminar Leipzig on Multigrid and Related Methods for Optimisation Problems, pp. 11–30 (2002)
- Cremers, D., Kohlberger, T., Schnörr, C.: Nonlinear shape statistics in mumford-shah based segmentation. In: A.H. et al. (ed.) 7th European Conference on Computer Vision, Copenhagen, Springer LNCS, vol. 2351, pp. 93–108 (2002)
- Cremers, D., Soatto, S.: Motion competition: A variational framework for piecewise parametric motion segmentation. Int. J. Comp. Vis. 62(3), 249–265 (2005)
- Cremers, D., Tischhäuser, F., Weickert, J., Schnörr, C.: Diffusion snakes: Introducing statistical shape knowledge into the mumfordshah functional. International Journal of Computer Vision 50(3), 1364–1379 (2002)

- Dacorogna, B.: Direct Methods in the Calculus of Variations. Appl. Math. Sciences 78. Springer–Verlag, Berlin (1989)
- Dal Maso, G., Morel, J., Solimini, S.: A variational method in image segmentation: existence and approximation results. Acta Math. 168, 89–151 (1996)
- Davatzikos, C.A., Bryan, R.N., Prince, J.L.: Image registration based on boundary mapping. IEEE Trans. Medical Imaging 15, no. 1, 112–115 (1996)
- De Giorgi, E., Carriero, M., Leaci, A.: Existence theorem for a minimum problem with free discontinuity set. Arch. Rat. Mech. and Anal. 108, 195–218 (1989)
- Delfour, M.C., Zolésio, J.: Geometries and Shapes: Analysis, Differential Calculus and Optimization. Adv. Des. Control 4. SIAM, Philadelphia (2001)
- Dibos, F., Séré, É.: An approximation result for the minimizers of the Mumford-Shah functional. Boll. Un. Math. Ital. 11A(1) (1997)
- Droske, M.: On variational problems and gradient flows in image processing. Ph.D. thesis, Universität Duisburg-Essen (2005)
- Droske, M., Ring, W.: A Mumford-Shah level-set approach for geometric image registration. Tech. rep., Universität Duisburg-Essen, Universität Graz (2005). Submitted
- Droske, M., Rumpf, M.: Multi scale joint segmentation and registration of image morphology. Submitted
- Droske, M., Rumpf, M.: A variational approach to non-rigid morphological registration. SIAM Appl. Math. 64(2), 668–687 (2004)
- 40. Evans, L.C., Gariepy, R.F.: Measure Theory and Fine Properties of Functions. CRC Press (1992)
- Feng, X., Prohl, A.: Analysis of gradient flow of a regularized Mumford-Shah functional for image segmentation and image inpainting. Mathematical Modelling and Numerical Analysis (1999)
- Féron, O., Mohammad-Djafari, A.: Image fusion and unsupervised joint segmentation using a hmm and mcmc algorithms. J. of Electronic Imaging (2004). To appear
- 43. Fried, M.: Image segmentation using adaptive finite elements. Tech. rep., University of Canberra, Australia (2003)
- Grenander, U., Miller, M.I.: Computational anatomy: An emerging discipline. Quarterly Appl. Math. LVI, no. 4, 617–694 (1998)
- 45. Hackbusch, W.: Multigrid Methods and Applications. Springer, Berlin/Heidelberg (1985)
- Hackbusch, W., Sauter, S.: Composite finite elements for the approximation of pdes on domains with complicated microstructures. Numerische Mathematik 75, 447–472 (1997)
- Henn, S.: A Levenberg-Marquardt scheme for nonlinear image registration. BIT Numerical Mathematics 43(4), 743–759 (2003)
- Hintermüller, M., Ring, W.: A second order shape optimization approach for image segmentation. SIAM Appl. Math 64(2), 442– 467 (2003)
- Hintermüller, M., Ring, W.: An inexact Newton-cg-type active contour approach for the minimization of the mumford-shah functional. J. Math. Imag. Vision 20, 19–42 (2004)
- Höllig, K., Reif, U., Wipper, J.: Weighted extended B-spline approximation of dirichlet problems. SIAM J. Num. Anal. 39(2), 442–462 (2001)
- Joshi, S.C., Miller, M.I.: Landmark matching via large deformation diffeomorphisms. IEEE Trans. Medical Imaging 9, no. 8, 1357–1370 (2000)
- 52. Kapur, T., Yezzi, L., Zöllei, L.: A variational framework for joint segmentation and registration. IEEE CVPR MMBIA (2001)
- Kass, M., Witkin, A., Terzopoulos, D.: Snakes: Active contour models. International Journal of Computer Vision 1, 321–331 (1988)
- Kirsch, A.: An Introduction to the Mathematical Theory of Inverse Problems, *applied mathematical sciences*, vol. 120. Springer Verlag, New York (1996)
- Maes, F., Collignon, A., Vandermeulen, D., Marchal, G., Suetens, P.: Multi-modal volume registration by maximization of mutual information. IEEE Trans. Medical Imaging 16, no. 7, 187–198 (1997)
- 56. Mikula, K., Sarti, A., Sgallari, F.: Handbook of Medical Image Analysis: Segmentation and Registration Models (J.Suri et al., Eds.), chap. Co-volume level set method in subjective surface

based medical image segmentation. Kluwer Academic/Plenum Publishers, New York (2004)

- 57. Miller, M., Trouve, A., Younes, L.: On the metrics and Euler-Lagrange equations of computational anatomy. Annual Review of biomedical Engineering **4**, 375–405 (2002). In print
- Modersitzki, J., Fischer, B.: Fast diffusion registration. Special Issue of Contemporary Mathematics, AMS (2000)
- Modersitzki, J., Fischer, B.: Curvature based image registration. JMIV 18(1) (2003)
- Monasse, P.: Contrast invariant registration of images. In: Proceedings of the International Conference on Acoustics, Speech and Signal Processing, Phoenix, Arizona, vol. 6, pp. 3221–3224 (1999)
- Morel, J., Solimini, S.: Variational models in image segmentation. Birkäuser (1994)
- Mumford, D., Shah, J.: Optimal approximation by piecewise smooth functions and associated variational problems. Comm. Pure Appl. Math. 42, 577–685 (1989)
- Osher, S.J., Fedkiw, R.P.: Level Set Methods and Dynamic Implicit Surfaces. Springer-Verlag (2002)
- Osher, S.J., Paragios, N.: Geometric Level Set Methods in Imaging, Vision and Graphics. Springer (2003)
- Osher, S.J., Sethian, J.A.: Fronts propagating with curvature dependent speed: Algorithms based on Hamilton–Jacobi formulations. J. of Comp. Physics 79, 12–49 (1988)
- Richardson, T.J., Mitter, S.K.: A variational formulation based edge focussing algorithm. Sadhana Acad. P. Eng. S. 22(4), 553– 574 (1997)
- Sauter, S., Stahn, N.: Composite finite elements and multi-grid. part i: Convergence theory in 1-d. Tech. Rep. Preprint, 11-01, University of Zürich (2001)
- Sethian, J.A.: Level Set Methods: Evolving Interfaces in Geometry, Fluid Mechanics, Computer Vision and Materials Sciences. Cambridge Univ. Press (1996)
- 69. Sokołowski, J., Zolésio, J.P.: Introduction to shape optimization. Springer-Verlag, Berlin (1992). Shape sensitivity analysis
- Thirion, J.P.: Image matching as a diffusion process: An analogy with maxwell's demon. Medical Imag. Analysis 2, 243–260 (1998)
- Tsai, A., Yezzi, A., Willsky, A.: Curve evolution implementation of the Mumford-Shah functional for image segmentation, denoising, interpolation, and magnification. IEEE Transactions on Image Processing 10(8), 1169–1186 (2001)
- Unal, G., Slabaugh, G.: Coupled PDEs for non-rigid registration and segmentation. In: IEEE Computer Society International Conference on Computer Vision and Pattern Recognition (CVPR) (2005)
- Vemuri, B., Ye, J., Chen, Y., Leonard, C.: Image registration via level-set motion: Applications to atlas-based segmentation. Medical Image Analysis 7, 1–20 (2003)
- 74. Viola, P.A., Wells III, W.: Alignment by maximization of mutual information. Tech. Rep. AITR-1548 (1995)
- Warnke, R.: Schnelle Löser für elliptische Randwertprobleme mit springenden Koeffizienten. Dissertation, Zürich (2003)
- Wells, W., Viola, P., Atsumi, H., Nakajima, S., Kikinis, R.: Multimodal volume registration by maximization of mutual information (1996)